Regional cerebral activation accompanies sympathoexcitation in women with polycystic ovary syndrome

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Abstract

**Context:** Polycystic ovary syndrome (PCOS) is associated with increased sympathetic nervous system (SNS) activation but the cerebral pathways involved are unclear.

**Objective:** To compare cerebral (blood oxygen level-dependent [BOLD] fMRI), pressor (blood pressure [BP], heart rate [HR]) and muscle sympathetic nerve activity (MSNA) responses to isometric forearm contraction (IFC) in women with PCOS and matched controls.

**Design:** Case-control study

**Setting:** Referral center

**Participants:** 20 subjects with PCOS (age 29.8 ± 4.8yrs, BMI 26.1 ± 4.9kg/ m²) and 20 age/BMI-matched controls (age 29.7 ± 5.0yrs, BMI 26.1 ± 4.8kg/ m²)

**Main outcome measures:** BP, HR, catecholamine and MSNA responses to 30% IFC. BOLD signal change modelled for blood pressure response to 30% IFC.

**Results:** Whilst HR and BP increased to a similar extent in both groups following IFC, MSNA burst frequency increased by 68% in the PCOS group (n=7) compared to 11.9% in controls (n=7) (p=0.002). Brain activation indexed by the BOLD signal in response to IFC was significantly greater in the PCOS group (n=15) compared to controls (n=15) in the right orbitofrontal cortex (p<0.0001). Adjustment for insulin sensitivity, but not hyperandrogenism, abolished these between-group differences.

**Conclusions:** Our study confirms enhanced sympathoexcitation in women with PCOS and demonstrates increased regional brain activation in response to IFC. The right orbitofrontal cortex BOLD signal change in women with PCOS is associated with insulin sensitivity. Further studies are warranted to clarify whether this may offer a novel target for cardiovascular risk reduction.
Précis

In women with PCOS, enhanced sympathoexcitation is accompanied by cerebral activation in the right orbitofrontal cortex that is influenced by insulin sensitivity.
Introduction

Polycystic ovary syndrome (PCOS) is a common metabolic disorder characterized by defects in insulin secretion and action. This leads to an increased risk of metabolic syndrome and disorders of glucose tolerance, including type 2 diabetes [1]. Women with PCOS also display a higher prevalence of cardiovascular risk markers, including dyslipidemia [2], hypertension [3] and endothelial dysfunction [4], although studies are yet to confirm if this leads to increased cardiovascular morbidity and mortality.

Sympathetic nervous system (SNS) activation may also contribute to this enhanced cardiometabolic risk [5], since conditions associated with chronic sympathoexcitation, such as obesity, hyperinsulinemia and obstructive sleep apnoea (OSA), are common in women with PCOS. In support of this, heart rate variability is altered [6-8] and heart rate and blood pressure recovery after exercise is delayed [9-10] in women with PCOS compared to matched controls, consistent with enhanced sympathetic stimulation and increased peripheral arterial resistance. Direct measurement of muscle sympathetic nerve activity (MSNA) by microneurography has also confirmed enhanced sympathetic outflow in women with PCOS compared with age- and BMI-matched controls [11-12].

The mechanisms by which this enhanced sympathetic activation occurs are not entirely clear, although both hyperinsulinemia [12] and hyperandrogenism [11] have been implicated. The origins of this activation are also uncertain, although the hypothalamus [13], brainstem [14] and higher brain centers [15] appear to be involved in regulating sympathetic tone in rodents. Contemporary imaging techniques, such as positron emission tomography [16-17] and blood oxygen level-dependent functional magnetic resonance imaging (BOLD fMRI) [18-20], facilitate neuroanatomical localization of these responses in humans, and have identified a
number of cortical and brainstem regions involved in this process. To our knowledge, similar studies have not been undertaken in metabolic disorders characterized by insulin resistance, including PCOS, in which compensatory hyperinsulinemia might be anticipated to amplify the cerebral responses to sympathoexcitation.

We hypothesized that women with PCOS would have evidence of sympathoexcitation accompanied by functional differences in higher brain centres. We therefore set out to compare cerebral (BOLD fMRI), pressor (blood pressure and heart rate) and MSNA responses to an isometric forearm contraction model of sympathoexcitation in women with PCOS and matched controls.
Materials and Methods

Participants

Patients with PCOS (n=20) were recruited from the endocrine clinic at the University Hospital of Wales, the endocrine clinic at Morriston Hospital, Swansea, and Morlais Medical Practice, Merthyr Tydfil. Diagnosis was made according to the Rotterdam criteria [21]. Congenital adrenal hyperplasia, Cushing’s syndrome, androgen-secreting neoplasms, hyperprolactinemia and thyroid disease were excluded by biochemical testing. Patients were aged between 18 and 45 years. Exclusion criteria were: pregnancy and breastfeeding, hyperlipidemia or use of lipid-lowering agents, hypertension or use of anti-hypertensives, use of glucocorticoids or anti-obesity drugs, diabetes or use of antidiabetic drugs within 3 months. Patients with any contraindication to MRI were also excluded. Of the 20 women, 12 had polycystic ovaries (PCO), hyperandrogenism and anovulation, 5 had hyperandrogenism and anovulation, 2 had PCO and hyperandrogenism, and 1 had PCO and anovulation.

Healthy volunteers (n=20) were recruited as controls. For each individual patient, a control was identified matched for age (within 2 yrs) and BMI (within 2 kg/m²). Controls needed to have regular menstrual cycles (menses every 27–32 days). Their healthy state was determined by history, examination and hormonal evaluation (testosterone, androstenedione, thyroid function, prolactin). Control subjects with signs of hirsutism or with a personal history of diabetes or hypertension, or a family history of PCOS, or current pregnancy were excluded. Those with any contraindication to MRI were also excluded. Healthy volunteers were recruited by advertisement among staff and students at the University Hospital of Wales, Cardiff University and in the local press. The study was approved by Cardiff University (study sponsors), Cardiff
and Vale University Health Board and the South East Wales Research Ethics Committee (reference 12/WA/0239). All subjects gave written, informed consent.

**Anthropometric and biochemical measurements**

Height, weight, waist and hip circumference were measured according to our previously published protocol [22]. Blood samples were collected after an overnight fast. Serum total cholesterol and triglycerides were assayed using an Aeroset analyzer (Abbott Diagnostics). Insulin was measured using an immunometric assay specific for human insulin (Invitron), and glucose was measured using the Aeroset chemistry system (Abbott Diagnostics). Total testosterone was measured by liquid chromatography-tandem mass spectrometry (QuattroTM Premier XE triple quadrupole tandem mass spectrometer; Waters Ltd). Androstenedione was measured by tandem mass spectrometry using an in-house method. Thyroid function tests were assayed using the Abbott Architect platform (Abbott Laboratories). HbA1c was determined using a high-performance liquid chromatography (HPLC) assay (Tosoh HLC-723G8, Tosoh Corporation). The intra- and inter-assay coefficients of variation were all <9%.

A standard 75-g oral glucose tolerance test was performed in all participants to determine post-prandial insulin sensitivity. Glucose and insulin were measured at 0, 30, 60, 90, and 120 minutes. The areas under the curve (AUCs) for insulin and glucose were calculated using the trapezoid method. The homeostatic model assessment (HOMA) method was also used to estimate fasting insulin resistance (HOMA-IR) according to the formula (fasting insulin (mU/L) x fasting glucose (mg/dL)/405) [23].
Isometric forearm contraction (IFC) protocol

Isometric forearm contraction (IFC) at 30% maximum voluntary contraction was used to generate a peripheral haemodynamic and SNS response. Maximum grip strength was determined by asking the volunteer to squeeze an electronic hand dynamometer (90kg capacity range) (Zhongshan Camry Electronic Co. Ltd, Guangdong, China) with their dominant hand to maximum effort on three separate attempts, with a 60 second period of rest between each squeeze, as previously recommended [24]. The mean maximum grip strength was determined and 30% IFC subsequently calculated. This was then applied in a protocol which followed a block design of 12 minutes in total, comprising 1 minute rest, 3 minutes squeeze, 2.5 minutes rest, 3 minutes squeeze and 2.5 minutes rest. The subjects were cued for the rest and squeeze periods, and targeted to sustain 30% IFC during the squeeze periods (figure 1).

Sympathetic activity measurements

Blood pressure and heart rate. Resting blood pressure (mmHg) and heart rate (beats/min) were measured at baseline using an Omron HEM-907 blood pressure monitoring device (Omron Healthcare UK Ltd) on the non-dominant arm and every 30 seconds throughout the 12 minute IFC protocol. Mean arterial blood pressure (MAP) was calculated. The mean of the values at rest were calculated as a pre-IFC blood pressure and heart rate, and the mean of values at the end of each 3 minute squeeze to give a post-IFC blood pressure and heart rate.

Plasma catecholamines. Blood was drawn from the non-dominant arm of the subject in a supine position after a 10 minute rest period (pre-IFC catecholamines). Following 3 minutes of IFC at 30% maximum handgrip strength, further blood was drawn for post-IFC
catecholamines. Samples were centrifuged at 2000rpm at 4°C within 10 minutes of collection and aliquots stored at -80°C until analysis. Catecholamines were measured using an Epinephrine ELISA Kit (Abnova, Taoyuan County, Taiwan) and Norepinephrine ELISA Kit (Abnova, Taoyuan County, Taiwan). The intra- and inter-assay coefficients of variation were <15.4% and <16.1% respectively.

Microneurography. A subset of patients (n=7, age 29.6 ± 6.4 yrs, BMI 27.3 ± 4.9 kg/m²) and controls (n=7, age 30.1 ± 6.2 yrs, BMI 27.1 ± 6.2 kg/m²) agreed to undergo microneurography. Studies were conducted on a separate day between 0830 and 1530 hours in a quiet physiological lab maintained at 20°C and performed by a single observer blind to subject status (YS). Direct recordings of multiunit efferent postganglionic muscle sympathetic nerve activity (MSNA) were obtained with a tungsten microelectrode with a tip diameter of a few micrometers inserted into a muscle fascicle of the peroneal nerve, posterior to the fibular head. A low-impedance reference electrode was inserted subcutaneously a few centimeters from the fibular head. When a muscle nerve fascicle was identified, small electrode adjustments were made until a site was found in which spontaneous, pulse-synchronous bursts of neural activity could be recorded. Details of the nerve recording technique and criteria for MSNA have been reported previously [25]. Bursts identified by inspection of the mean voltage neurogram were expressed as burst frequency (number of pulse synchronic sympathetic bursts per minute) [bursts/min (BF)] and burst incidence (number of pulse synchronic sympathetic bursts per 100 heart beats) [bursts/100 heartbeats (BI)]. Total MSNA activity was measured to take into account both the
frequency and size of a sympathetic burst (the product of burst per minute and mean burst amplitude), expressed in arbitrary units. The total MSNA during the last 60 seconds of a rest period was used as a baseline to establish the percentage change in MSNA during the last 60 seconds of the 30% IFC.

MRI data acquisition

MRI was performed on a 3T GE HDx MRI system (General Electric). The head was held immobile in an eight-channel receive only head coil by foam pads. A continuous series of 232 fMRI image volumes (echo-planar images using BOLD contrast, scan time = 12 mins, TR = 3.1s, TE = 25ms) were collected for each run. In-plane voxel size was 1.5x1.5 mm$^2$, matrix 128x128x40 and Field-of-view (FOV) 192x192mm$^2$ in plane. The slice thickness was 2.2mm and slice gap 0.8mm. Each volume covered the entire brain and brainstem. Slices were tilted 10°-15° from the axial to the coronal plane to reduce signal loss due to dephasing in the brainstem resulting from through-slice susceptibility-induced gradients [26]. Structural images were collected using a T1-weighted sequence in order to facilitate visualization.

Blood oxygen level-dependent (BOLD) fMRI scan protocol

The scan protocol aimed to reveal BOLD signal correlates with the IFC task, using a block design. Subjects were fitted with a nasal cannula to measure end tidal CO$_2$. Respiration pattern was determined by a strain-gauge band around the chest. Heart rate was measured from a pulse oximeter on the left hand (MedRad, USA). Physiological data were collected with a computer-
based data acquisition and analysis system (CED 1401, Cambridge, UK). An in-house MRI-compatible handgrip device was positioned in the dominant hand and connected to a pressure transducer. The pressure signal was collected with a computer-based data acquisition and analysis system (CED 1401, Cambridge, UK) and displayed on a screen located inside the scanner. Subjects followed visual instructions presented on the screen as to the rest and squeeze periods, with a target bar showing when 30% squeeze had been achieved. PsychoPy version 1.78 [27] was used to run the visual stimulus. Subjects performed the previously described block paradigm twice with time to rest between the runs.

**Image and statistical analyses**

Analysis of the scans was by FEAT (fMRI Expert Analysis Tool, version 6.00) software (available on-line at www.fmrib.ox.ac.uk/fsl). Each T1 scan was registered to the MNI152, an average T1 brain image constructed from 152 normal subjects at the Montreal Neurological Institute (MNI), Montreal, QC, Canada, using linear registration (FLIRT within the FMRIB Software Library (FSL)) [28-29]. The functional BOLD scans were then registered to each individual’s T1 structural image. fMRI images were un-warped, motion corrected and spatially smoothed. Physiological noise from cardiac and respiratory signals was retrospectively regressed out from the images. FSL contains the software FLIRT (FMRIB’s Linear Image Registration Tool) that allowed the linear transformation of imaging data [28, 30]. A high-pass filter of 330 seconds was used. To generate contrast images, task-related BOLD activation was estimated with a design matrix specifying a general linear model (GLM) that included a waveform based on each person’s IFC recording obtained during the scan protocol from the handgrip device. The visual stimulus shown in the scan session was also included in this analysis. BOLD signal changes for blood pressure condition were modelled with a waveform derived from the blood pressure recordings made out of scanner during the 12-minute
paradigm. Z statistic images were thresholded using clusters determined by $z > 2.3$ and a cluster significance threshold of $P = 0.05$ [31]. Significant BOLD signal intensity changes were color coded and rendered onto an individual’s T1-weighted anatomic image set. The resulting statistical parametric maps were used in higher level analysis to determine differences between PCOS and control groups. As the paradigm was run twice, an intermediate level FEAT analysis was run for each subject by combining their two lower-level FEAT outputs, to produce an average for each subject. These were then used in the higher-level FEAT analysis that could be used in the group analyses to examine BOLD activation in the PCOS and control groups and the differences in activation between groups ($z > 2.3$, $p=0.05$).

For the pressor, MSNA and catecholamine responses, statistical analysis was performed using SPSS version 20.0 (IBM, New York). An independent-samples t-test was used to compare the difference between the PCOS and control group means. A p-value of <0.05 was considered statistically significant.
Results

Baseline characteristics

Table 1 shows the clinical, anthropometric and metabolic characteristics of the two groups. The groups were closely matched for age, BMI, resting heart rate and blood pressure. Testosterone and androstenedione levels were non-significantly higher in PCOS subjects than controls. Similarly, the insulin response to oral glucose challenge (insulin AUC) and HOMA-IR values were higher in PCOS subjects but fell just short of statistical significance. Triglyceride levels in the PCOS group were higher than in controls.

Sympathetic activity measurements

Pressor response

19 PCOS and 19 controls had heart rate (HR) and blood pressure (BP) measured in response to the IFC paradigm (table 2). As anticipated, IFC induced a significant rise in HR and BP in both groups. However, there were no between-group differences in the HR or BP increase from baseline in response to IFC.

Catecholamines

The plasma catecholamine response to IFC was assessed in 39 subjects (20 PCOS, 19 controls) (table 2). Mean resting catecholamine concentrations were not different between groups. Following IFC, norepinephrine levels did not change but epinephrine concentrations increased significantly in the PCOS group (p<0.001). However, differences between groups in epinephrine response to IFC were not apparent.
Resting data were obtained from 16 subjects (8 PCOS, 8 controls). Only 14 of these (7 PCOS, 7 controls) were able to proceed with full MSNA recordings post-IFC due to technical difficulties, including inability to locate the peroneal nerve for recordings (n=1) and a participant who was unable to keep their leg in position (n=1).

Resting burst frequency (BF), burst incidence (BI) and total MSNA was not different between groups (table 2). The increase in BF was significantly greater (68%) in the PCOS group compared to controls (11.9%; p=0.002). The increases in BI (PCOS: 55.4%, controls: 20.5%) and total MSNA (PCOS: 124.1%, controls: 86.4%) were not significantly different between groups.

**fMRI BOLD signal activation**

30 participants (15 PCOS, 15 controls) underwent fMRI scanning with out-of-scanner HR and BP changes recorded every 30 seconds in response to the IFC paradigm. There were no significant differences in the age, BMI, testosterone, HOMA-IR, resting HR or resting BP between groups. The change in BOLD signal intensity that fitted the modelled blood pressure response showed activation in the PCOS group in the right cerebral cortex, right pallidum, right thalamus and right parietal operculum cortex (p<0.0001) and control group in the intracalcarine cortex and lingual gyrus (p=0.003). BOLD signal activation was significantly greater in the PCOS group compared to controls in the right orbitofrontal cortex (p<0.0001), and less so in the left angular gyrus and lateral occipital cortex (p=0.04) (figures 2(a) and 2(b)). No differences were observed in the brainstem.

**Metabolic influences on fMRI BOLD signal change**
When the BOLD signal change modelled for hemodynamic response was adjusted for variance associated with testosterone, using testosterone as a covariate at the group level, BOLD activation in the right orbitofrontal cortex was still greater in the PCOS group compared to controls (p<0.0001). However, when the BOLD signal was separately adjusted for insulin sensitivity (HOMA-IR), the BOLD signal differences between groups in the right orbitofrontal cortex were no longer significant. When corrected for HOMA-IR, the BOLD signal in the left angular gyrus and lateral occipital cortex remained significant.
Discussion

Our study demonstrates that women with PCOS have evidence of enhanced sympathoexcitation in response to IFC compared to age- and BMI-matched controls, and that this is accompanied by a difference in BOLD signal change that localizes to the right orbitofrontal cortex. This finding is consistent with previous studies implicating this region in the neural control of blood pressure [17, 32, 33], but to our knowledge is the first to confirm enhanced activation in this region in young women with insulin resistance. These observations may extend our understanding of the mechanisms involved in neurogenic hypertension in young ‘at risk’ subjects.

In common with many previous studies, we used IFC at 30% of maximum grip as our stimulus to induce a blood pressure rise. In young adult volunteers this has been shown not to increase nociception [18]. The pressor response we observed was of a similar magnitude to other studies [18, 34-35] and did not differ between women with PCOS and controls. This is in keeping with observations in patients with type 2 diabetes whereby systolic and diastolic blood pressure rose in parallel to controls in response to IFC, despite differences in resting blood pressure between groups [36].

We did not observe any rise in concentrations of the sympathetic neurotransmitter norepinephrine in either group but plasma measurement offers limited sensitivity and reproducibility, unlike radiolabelled techniques which may be used reliably to measure regional sympathetic activity in individual organs. Furthermore, plasma norepinephrine measurement cannot distinguish between increased central catecholamine production and
reduced clearance [37]. For these reasons, the significance of the greater rise in plasma epinephrine concentrations in the PCOS group following IFC is uncertain.

In contrast to plasma catecholamines, microneurography represents a more direct measurement of sympathetic neural output. In common with many studies, we chose the common peroneal nerve, in view of its easy accessibility, to measure efferent MSNA. Importantly, MSNA correlates well with autonomic effector (including blood pressure and heart rate) responses [25], and provides immediate data on sympathetic output. However, it is invasive, hence we were only able to recruit a proportion of our total group to this sub-study. Nevertheless, women with PCOS showed a greater rise in burst frequency in response to IFC than controls, although resting measures were not different between groups. This contrasts with previous studies, where higher resting MSNA values were observed in women with PCOS [11-12]. However, it is noticeable that the resting burst frequency and burst incidence values in our control group were significantly greater than those reported in these previous studies, and this may go some way to explain the absence of differences in MSNA between our two groups at baseline.

This study identified several cortical areas whose BOLD signal change correlated with the modelled BP response to static exercise. Of these, between-group differences were most apparent in the right orbitofrontal cortex. This cerebral region has previously been shown to associate with a pressor response in humans. In a positron emission tomography study, Critchley and colleagues identified the right orbitofrontal cortex as one of several brain regions implicated in the cardiovascular response to isometric exercise and mental stress [17]. Harper et al. used functional MRI to demonstrate increased activity in the right orbitofrontal cortex during hypertension induced by cold pressor and Valsalva stimuli [33], whilst Gianaros et al. showed that the orbitofrontal cortex was similarly activated in response to a behavioral stressor
More recently, Macefield and Henderson contemporaneously captured skin sympathetic nerve activity (SSNA) directly during BOLD fMRI of the brain [38], showing correlation of spontaneous SSNA with BOLD signal intensity in the right orbitofrontal cortex. Furthermore, in animal studies, the orbitofrontal cortex has been shown to connect to the insular cortex, a key regulator in the pressor response [39]. Our data therefore support the prevailing view that a cortical and sub-cortical network exists in humans to control cardiovascular responses. Studies in patients with intractable epilepsy undergoing intracranial electrode implantation and deep brain stimulation appear to confirm this, whereby stimulation of the subcallosal neocortex, which lies adjacent to the orbitofrontal cortex, elicited marked systolic hypotensive changes likely as a result of reduced sympathetic drive [40].

In an attempt to understand the potential metabolic drivers of the altered BOLD signal response, we extended our analyses to sequentially adjust for hyperandrogenism and insulin resistance, observing that adjustment for HOMA-IR, but not testosterone, abolished the between-group differences in BOLD signal intensity in the right orbitofrontal cortex. This implies that differences in insulin sensitivity, and compensatory hyperinsulinemia, might account for the differences we observed in the BOLD signal response in this area in response to IFC. Our findings may thus have relevance for other metabolic disorders characterized by insulin resistance, such as metabolic syndrome and type 2 diabetes, which we speculate might similarly be affected by altered BOLD signal in this cerebral region. Although little insulin is produced in the brain, insulin receptors are widely distributed in the brain and peripherally-made insulin can cross the blood-brain barrier [41]. Furthermore, intracerebroventricular injection of insulin in rodents induces sympathoexcitation via the arcuate nucleus [13, 42]. In humans, hyperinsulinemia increases MSNA and modifies baroreflex control of sympathetic activity [43-44] although these effects of insulin on sympathetic outflow may be blunted in
insulin-resistant states such as obesity and the metabolic syndrome [45-46]. We therefore speculate that the enhanced activation observed in the right orbitofrontal cortex in women with PCOS may reflect preserved insulin sensitivity in this cerebral region. This raises the possibility that insulin sensitization might have therapeutic benefit in reducing sympathetic output in PCOS and consequently improving cardiometabolic outcomes. Indeed, metformin caused a dose-dependent reduction in heart rate, blood pressure and renal sympathetic nerve activity in spontaneously hypertensive rats [49], but similar benefits were not observed short-term in obese hypertensive men [50]. In contrast, both rosiglitazone and pioglitazone have been shown to reduce sympathetic nerve activity in subjects with type 2 diabetes [51-52].

In contrast to other studies [18], we did not find any change in BOLD signal in the brainstem following IFC, a region that we hypothesized at the outset might be activated in response to this paradigm. In particular, medullary structures are implicated in autonomic control of cardiovascular responses. Reasons for this might include physiological noise due to cardiac and respiratory motion, and the presence of magnetic field inhomogeneity caused by the nearby sphenoid sinus. Furthermore, the small size of brainstem nuclei in humans [53] makes localization challenging even when using MRI scanners (3T) that image with greater resolution than conventional systems. In this regard, the enhanced signal and spatial resolution offered by 7T systems may offer an important advance.

Our study has some limitations. Firstly, we chose to define our subjects with PCOS by the Rotterdam criteria since this embraces a ‘milder’ metabolic phenotype characterized by lesser degrees of hyperandrogenism and insulin resistance than other definitions such as the NIH criteria [54]. Whilst this allowed us to explore the effects of relatively mild insulin resistance on cerebral and pressor responses to IFC, the study group was heterogeneous and it is difficult
to be certain if our findings extend to all sub-phenotypes of the syndrome; further studies are needed in this regard. Since patients with hyperandrogenic PCOS carry a worse cardiometabolic risk profile, we speculate that inclusion of patients with more severe hyperandrogenism may have exaggerated the differences we observed in orbitofrontal cortex activation and/or unmasked other cerebral regions implicated in the neurogenic regulation of blood pressure. Inclusion of a young population nevertheless avoids the potentially confounding influences of vascular pathology (from e.g. diabetes and hypertension) on blood flow and therefore BOLD signal. Secondly, MSNA and pressor recordings were undertaken out-of-scanner; it would have been preferable to do so during scanning, as demonstrated recently by others [20, 38] but this is beyond our current technical ability. Thirdly, our study used static hand grip to induce a pressor response, which is a motor task cued by a visual stimulus. Although the potential confounding influence of this model was reduced by factoring the motor and visual tasks into the FEAT analysis, we nevertheless observed a change in BOLD signal intensity in the intracalcarine cortex and lingual gyrus in controls, in the parietal operculum in subjects with PCOS, and between-group differences in the lateral occipital cortex and left angular gyrus, which are likely to relate to remaining confounding effects of the visual stimulus. Similarly, the signal change in the right thalamus, pallidum and cerebral cortex in the PCOS group may reflect residual confounding by the motor component of the hand grip task. However, imaging studies have also suggested that areas of the thalamus may be implicated in blood pressure control, potentially via increasing vagal tone and reducing sympathoexcitation [55].

In conclusion, our study supports previous observations of enhanced sympathetic output in women with PCOS but demonstrates for the first time that this is accompanied by regional differences in cerebral activation that are most marked in the right orbitofrontal cortex. This
Differential activation appears to relate to altered insulin sensitivity, and suggests that treatments targeted at reducing hyperinsulinemia in young women with PCOS may have benefits in reducing sympathetic output and improving cardiovascular health.

References


and endothelial dysfunction in polycystic ovary syndrome are not explained by either obesity or insulin resistance. *Clin Endocrinol (Oxf).* 2015; 83(6): 812-9.


### Table 1. Anthropometric and metabolic characteristics of the study population

<table>
<thead>
<tr>
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<th>PCOS (n=20)*</th>
<th>Control (n=20)</th>
<th>p-value</th>
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<tbody>
<tr>
<td><strong>Age (yrs)</strong></td>
<td>29.80 ± 4.78</td>
<td>29.65 ± 4.96</td>
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<tr>
<td><strong>BMI (Kg/m²)</strong></td>
<td>26.05 ± 4.90</td>
<td>26.11 ± 4.83</td>
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<td><strong>WHR</strong></td>
<td>0.88 ± 0.07</td>
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<td><strong>Waist circumference (cm)</strong></td>
<td>85.9 ± 13.7</td>
<td>85.1 ± 11.1</td>
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<tr>
<td><strong>Hip circumference (cm)</strong></td>
<td>97.2 ± 10.4</td>
<td>101.4 ± 11.8</td>
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<td><strong>Testosterone (nmol/L)</strong></td>
<td>1.41 ± 0.77</td>
<td>1.03 ± 0.53</td>
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<tr>
<td><strong>Androstenedione (nmol/L)</strong></td>
<td>4.51 ± 2.99</td>
<td>3.64 ± 1.28</td>
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<td><strong>HbA1c (mmol/mol)</strong></td>
<td>34.15 ± 2.76</td>
<td>34.21 ± 2.64</td>
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<td><strong>Total cholesterol (mmol/L)</strong></td>
<td>5.22 ± 1.05</td>
<td>4.79 ± 0.55</td>
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<td><strong>Triglycerides (mmol/L)</strong></td>
<td>1.34 ± 0.68</td>
<td>0.90 ± 0.36</td>
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<td><strong>Insulin AUC (pmol min/L)</strong></td>
<td>55519.50 ± 41547.67</td>
<td>35320.26 ± 21008.31</td>
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<td><strong>Glucose AUC (mmol min/L)</strong></td>
<td>764.85 ± 239.02</td>
<td>661.89 ± 219.03</td>
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<td><strong>HOMA-IR</strong></td>
<td>1.41 ± 1.10</td>
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<td><strong>Resting HR (beats/min)</strong></td>
<td>71.05 ± 8.59</td>
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<td><strong>Resting SBP (mmHg)</strong></td>
<td>114.53 ± 9.33</td>
<td>117.58 ± 12.62</td>
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<td><strong>Resting DBP (mmHg)</strong></td>
<td>65.16 ± 13.33</td>
<td>65.47 ± 14.31</td>
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<td><strong>Resting MAP (mmHg)</strong></td>
<td>81.63 ± 11.26</td>
<td>83.84 ± 10.54</td>
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BMI, body mass index; AUC, area under the curve during oral glucose tolerance test;
HOMA-IR, homeostatic model assessment of insulin resistance. *19 controls underwent an oral glucose tolerance test.
Table 2. Pressor, catecholamine and MSNA responses to IFC in PCOS and control groups

<table>
<thead>
<tr>
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<th>PCOS Mean ± SD</th>
<th>Controls Mean ± SD</th>
<th>p-value PCOS vs controls</th>
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<tbody>
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<td></td>
<td>Pre-IFC</td>
<td>Post-IFC</td>
<td>p-value</td>
</tr>
<tr>
<td>Pressor response</td>
<td>n=19</td>
<td></td>
<td></td>
</tr>
<tr>
<td>HR (beats/min)</td>
<td>71.05 ± 8.59</td>
<td>76.68 ± 8.04</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>SBP (mmHg)</td>
<td>114.53 ± 9.33</td>
<td>127.11 ± 13.69</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>DBP (mmHg)</td>
<td>65.16 ± 13.33</td>
<td>74.84 ± 15.79</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>MAP (mmHg)</td>
<td>81.63 ± 11.26</td>
<td>92.37 ± 13.97</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Catecholamines</td>
<td>n=20</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Epinephrine</td>
<td>0.68 ± 0.53</td>
<td>1.23 ± 0.71</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>concentration (ng/mL)</td>
<td>18.11 ± 11.18</td>
<td>16.77 ± 10.01</td>
<td>0.38</td>
</tr>
<tr>
<td>Norepinephrine</td>
<td>25.9 ± 4.4</td>
<td>42.9 ± 8.2</td>
<td>0.001</td>
</tr>
<tr>
<td>concentration (ng/mL)</td>
<td>36.3 ± 9.9</td>
<td>54.4 ± 12.1</td>
<td>0.004</td>
</tr>
<tr>
<td>MSNA</td>
<td>n=7</td>
<td></td>
<td></td>
</tr>
<tr>
<td>BF (bursts/min)</td>
<td>2.4 ± 1.3</td>
<td>5.5 ± 3.1</td>
<td>0.004</td>
</tr>
</tbody>
</table>
HR, heart rate; SBP, systolic blood pressure; DBP, diastolic blood pressure; MAP, mean arterial pressure; MSNA, muscle sympathetic nerve activity; BF, burst frequency; BI, burst incidence.

Legends for figures

Figure 1. 12 minute IFC paradigm comprising 1 minute rest, 3 minutes 30% IFC, 2.5 minutes rest, 3 minutes 30% IFC and 2.5 minutes rest. The timings of MSNA, catecholamine, heart rate and blood pressure measurements are indicated.

Figure 2. BOLD signal activation (modelled for blood pressure) differences between PCOS and controls in the right orbitofrontal cortex (a) and between PCOS and controls in the left angular gyrus and lateral occipital cortex (b). The significant region is displayed with a threshold of $Z>2.3$, with a cluster probability threshold of $p<0.05$. 
Time (minutes)

< 1 >  < 3 >  < 2.5 >  < 3 >  < 2.5 >

% of maximum IFC

0%  30%

HR and BP

Catecholamines

MSNA